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## A biologically inspired algorithm to deal with filter-overlap in retinal models

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### Introduction

A multi-filter LN retinal model to simulate parallel processing by a population of retinal ganglion cells was proposed in [1] to test rank-order codes [2], a spike-latency based neural code. Dealing with filter-overlap in this model has been an area of concern [3,4]. This is because data redundancy induced by over-sampling of a point in space affects the quantity of salient information during rapid information transmission [5]. We propose a Filter-overlap Correction algorithm (FoCal) to deal with this problem of over-sampled data. The algorithm is based on the lateral inhibition technique [6] used by sensory neurons to deal with data redundancy [7], so that only salient information is transmitted through the optic-nerve bottleneck for rapid object detection and recognition.

Following the seminal work in [6] on lateral inhibition, mutual inhibition was described quantitatively in [8] as

$$r_1 = e_1 - K_{1,2}(r_2 - r_{1,2}^0) \quad r_2 = e_2 - K_{2,1}(r_1 - r_{2,1}^0),$$

where  $r$  is the response of a receptor unit,  $e$  is the excitation supplied by the external stimulus on the receptor,  $K$  is the coefficient of inhibitory influence of one receptor over the other, and  $r^0$  is the threshold frequency. Let  $\Phi_1$  and  $\Phi_2$  be two filters sampling an image at spatial locations  $(x, y)$  and  $(x+1, y)$  respectively on a digital raster, the respective coefficients of filtering  $c_1$  and  $c_2$  representing the spiking latency of the retinal ganglion cells corresponding

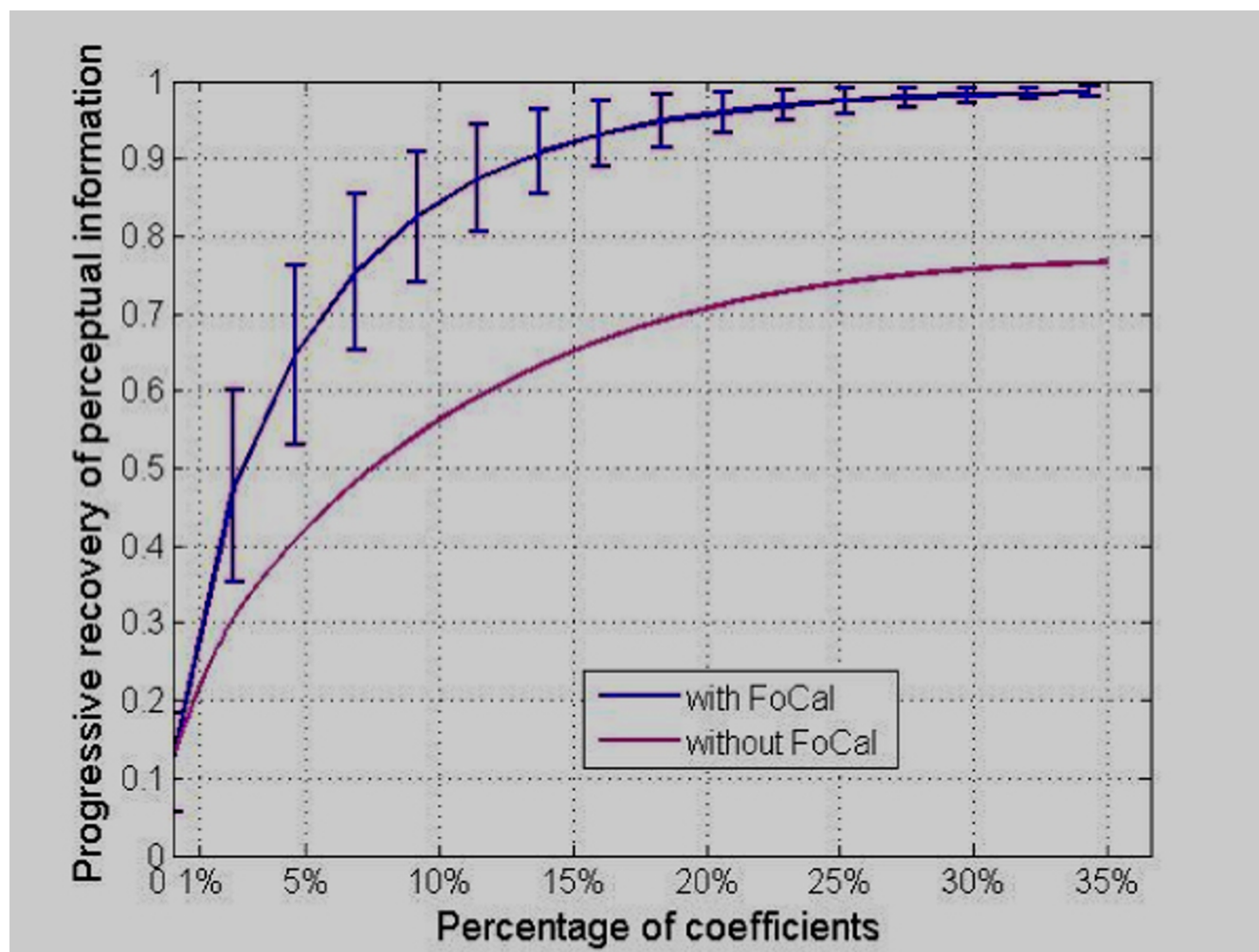
to the filters. The filter overlap is written as  $O_{1,2} = O_{2,1} = \langle \Phi_1, \Phi_2 \rangle$ . Let  $c_1 > c_2$ . The smaller coefficient is corrected for the effect of this overlap thus

$$r_2 = c_2 - O_{2,1} \cdot c_1,$$

where  $r_2$  simulates the overlap corrected response latency of the ganglion cell corresponding to  $\Phi_2$ . However, we introduce lateral inhibition post-spiking whereas it is pre-spiking in biology. Thus, we substitute the stimulus strength  $e_2$  with the corresponding coefficient of filtering  $c_2$ . The threshold frequency is also irrelevant in our case. Further, we implement a winner-take-all mechanism in each iteration of the algorithm: the largest coefficient inhibits all others, the degree of inhibition being proportional to  $O$ , which corresponds to  $K$ . This reduces redundancy in the coefficient set and helps prioritise salient information, thus enabling rapid recovery of perceptually important information [4] in rank-order encoded images.

### Results and conclusion

Using a data set of 65 images, we obtain the mean perceptually-important information recovery plot as shown (Figure 1). The error-bars show the standard deviation across the data set. We observe an increase of more than 20% in the total information recovered. Moreover, the rate of information recovery is much faster, with 80% recovery using the top 10% of the coefficients, which is a 30% increase compared to rank-order encoding without using FoCal. Based on these results, we argue that FoCal pro-



**Figure 1**

vides a general method for coping with non-orthogonal basis functions for current and future biologically inspired visual models.

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